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Nail drug delivery using different formulations and different model systems

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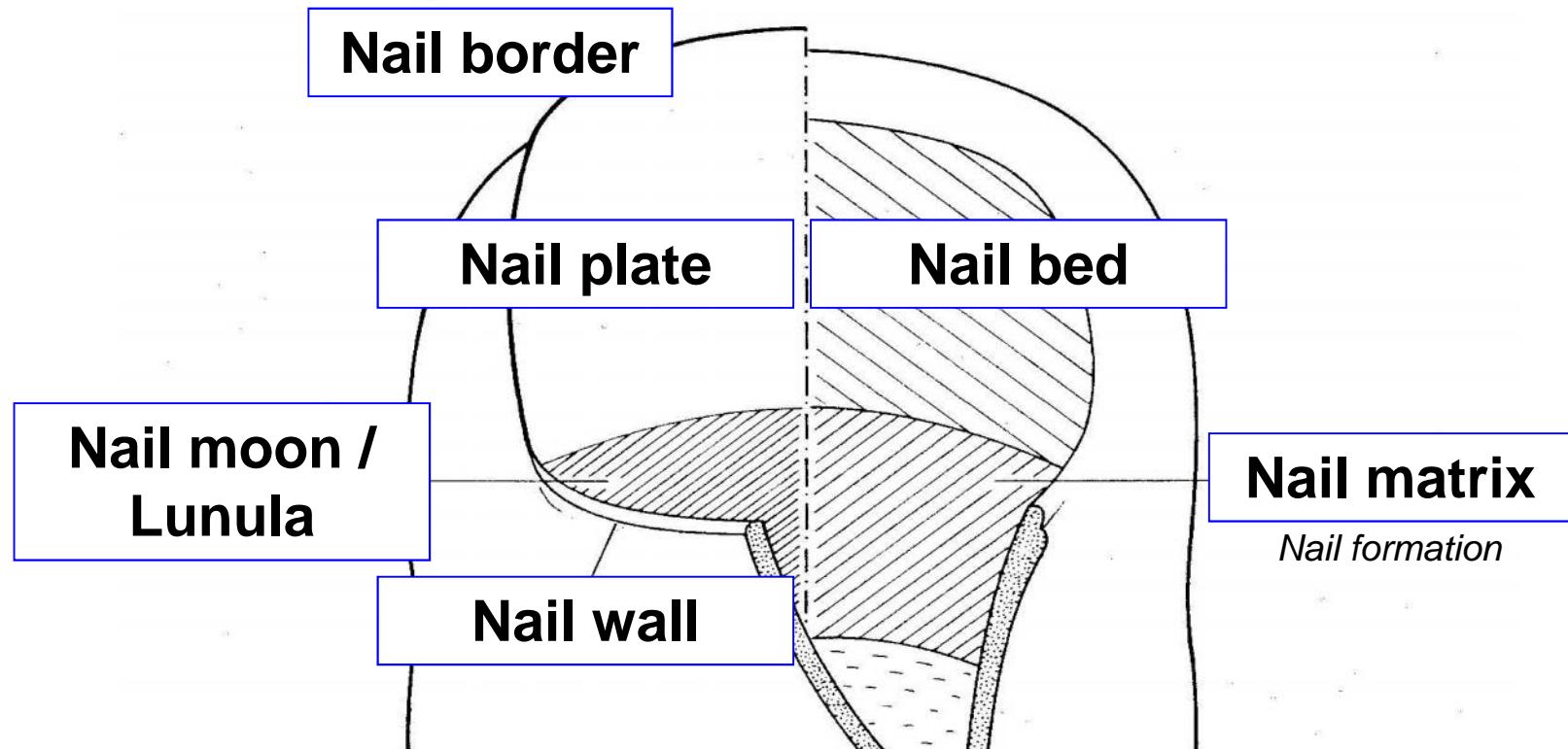
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- 3. Onychomycosis and antimycotic drug EV-086K**
- 4. Different formulations for EV-086K**
- 5. Penetration of drugs through bovine and equine hoof and into human nails**
- 6. Comparison of the penetration data**
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Introduction

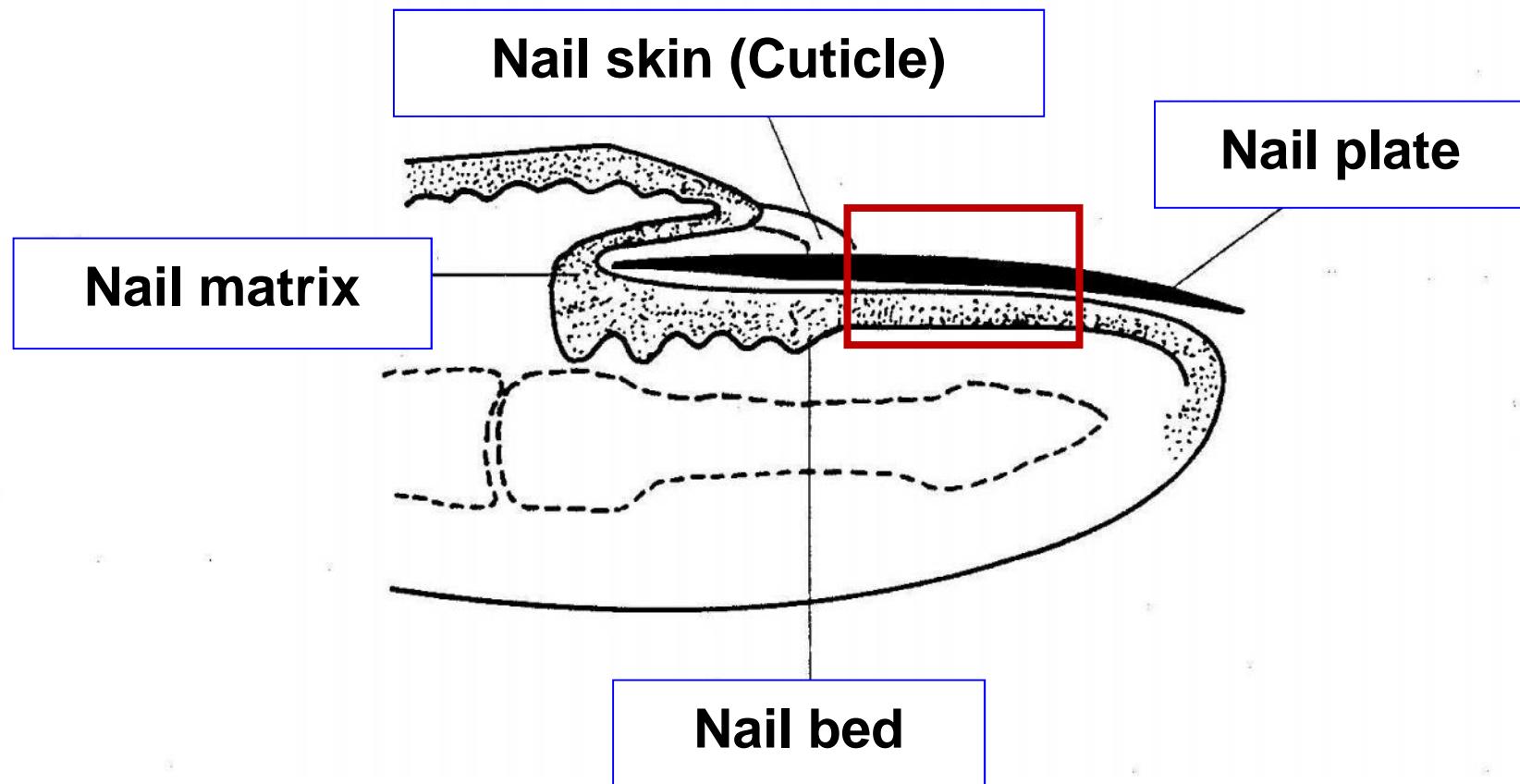
Anatomy nail (top view)





Introduction

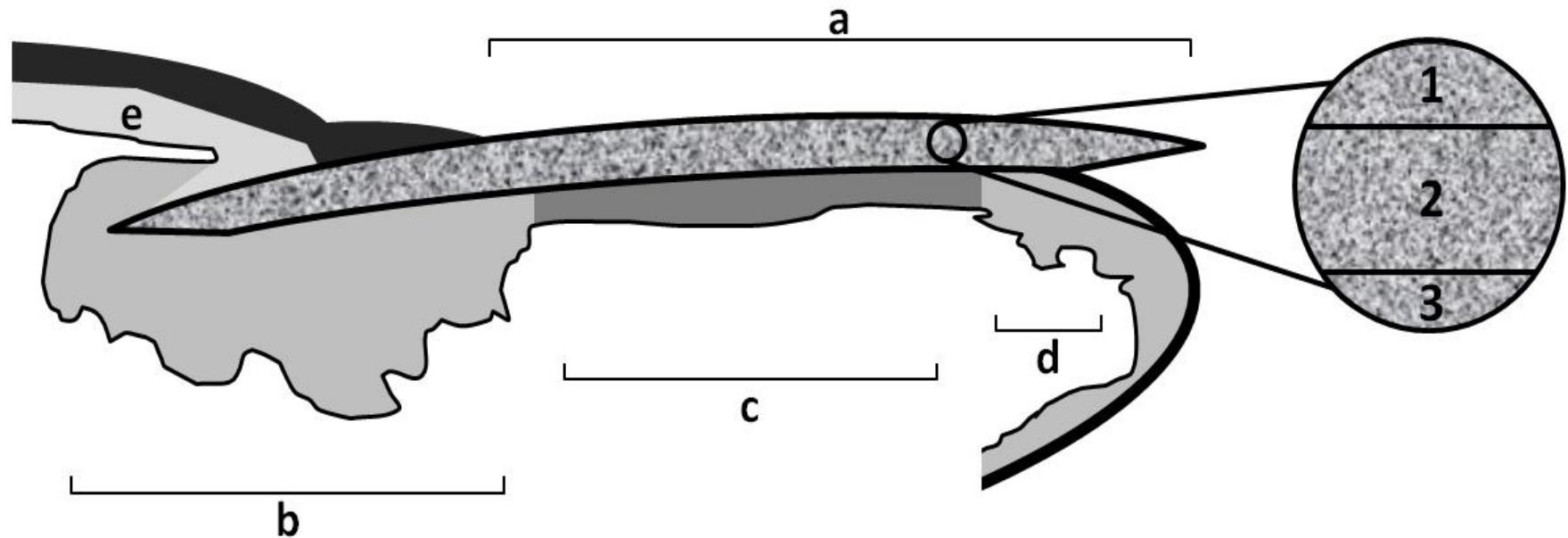
Nail Anatomy (lateral view)





Introduction

Nail Anatomy (lateral)



a = nail plate (1 = dorsal, 2 = intermediate, 3 = ventral nail plate)
b = nail matrix, c = nail bed, d = hyponychium, e = proximal nail fold



Physiologic conditions of the nails

Properties	SC	Nail
Thickness	10-40 µm	50 – 1000µm
Disulfide linkages	1.2%	10.6%
Lipid content	10-20%	0.1-1%
Water content	1-2% (up to 5%)	10-20% (up to 25%)
TEWL/TOWL	1.17-3.35 mg/cm ² /h	1.3-1.9 mg/cm ² /h
Behaviour	Lipophilic partition membrane	Concentrated hydrogel





Physiologic conditions of the nails

Nails: Hydrophilic gel membrane

- Thermal movement of the keratine fibers create wholes (pores) which would used as pathway for drugs as diffusion way
→ small molecules diffuses faster compared to larger ones
- Molecule size much smaller than pore size – convection and diffusion

Aqueous pathway dominant

- For extremely lipophilic substances: lipophilic pathway is discussed but special formulations are necessary





Onychomycosis

- Most relevant disease of nails: **Onychomycosis**
- Most relevant topical formulations: **Lacquers**
- **Scientific deficiencies:**
 - Studies according to drug liberation from lacquers and drug penetration/diffusion into the nails.
- **Problems:**
 - Model systems are needed to optimise drug liberation and penetration !





Onychomycosis

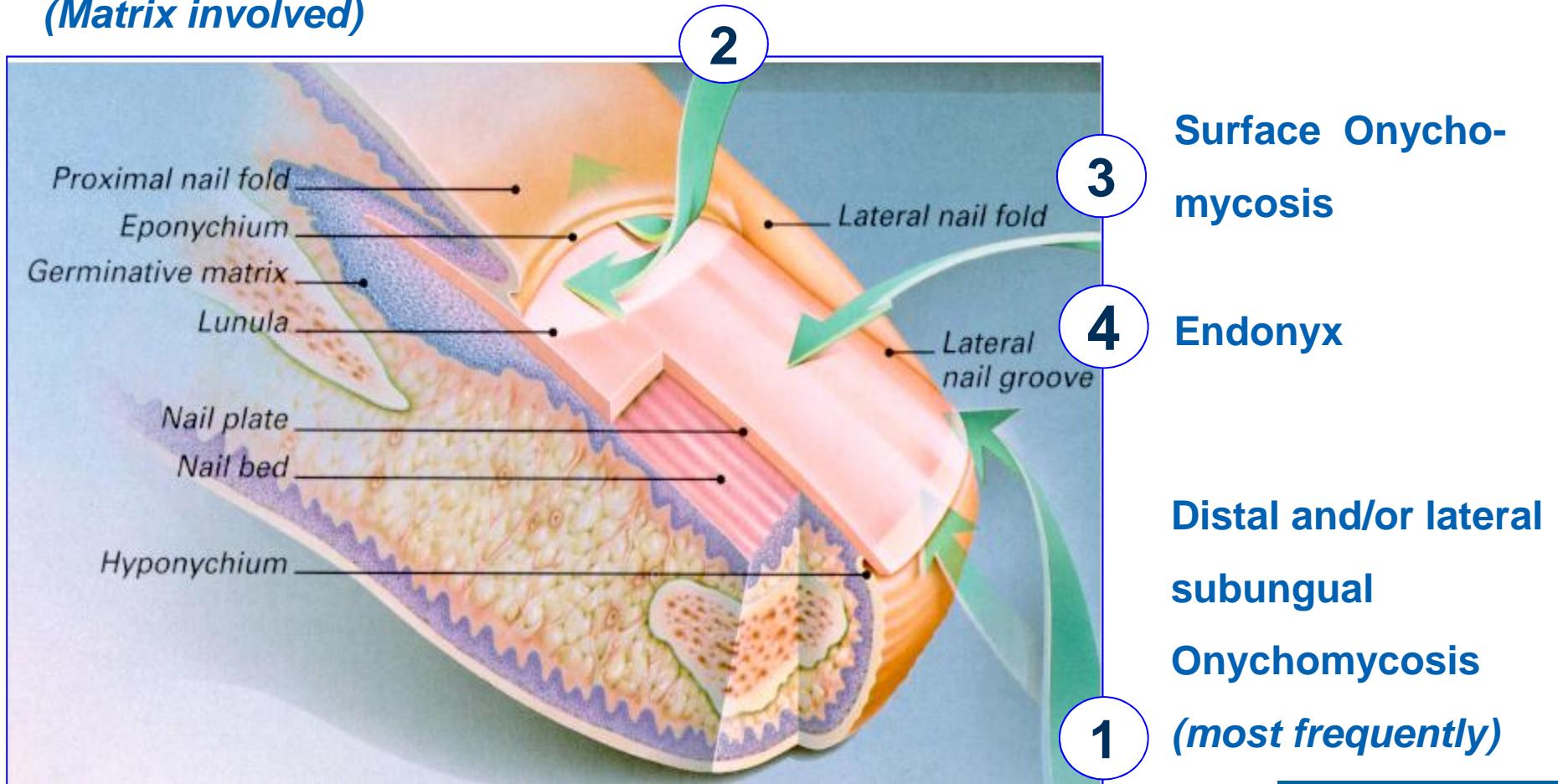
- **Onychomycosis** = chronic fungal infection of the nail apparatus, particularly the nail plate and the nail bed
- European Achilles foot screening project (n = 13486):
Prevalence in the population **8 to 23 %**
- **Problems:**
 - Long term treatment
 - High recurrence rate
 - Low patient compliance
- **Standard therapy:**
 - Terbinafine systemically
 - Amorolfine and ciclopirox topically (lacquers)





Onychomycosis

Proximal subungual Onychomycosis *(Matrix involved)*





Diffusion/Penetration set up

- **Online FTIR-ATR diffusion cell:**
 - ***Bovine hoof***
 - ***Equine hoof***
 - sliced into sections (approx. 60 – 150 µm)
- **Modified Franz diffusion cell:**
 - ***Human cadaver nail***
 - slicing of the nail plate using microtome

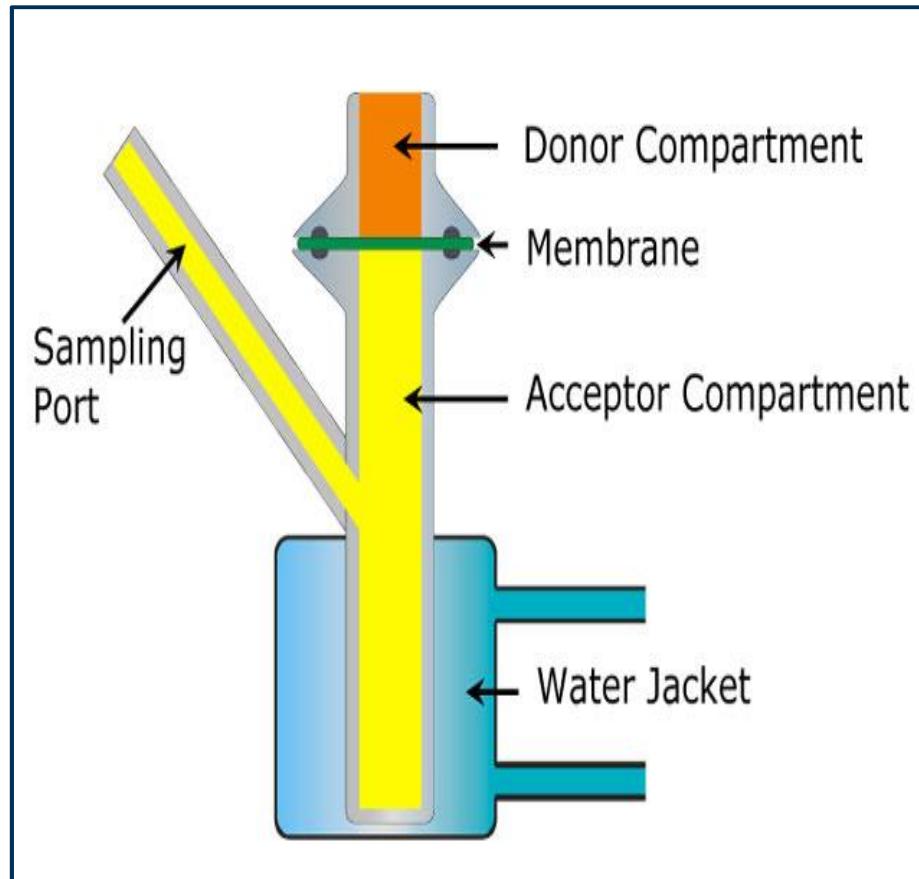




FRANZ & FTIR-ATR diffusion cell

Franz diffusion cell:

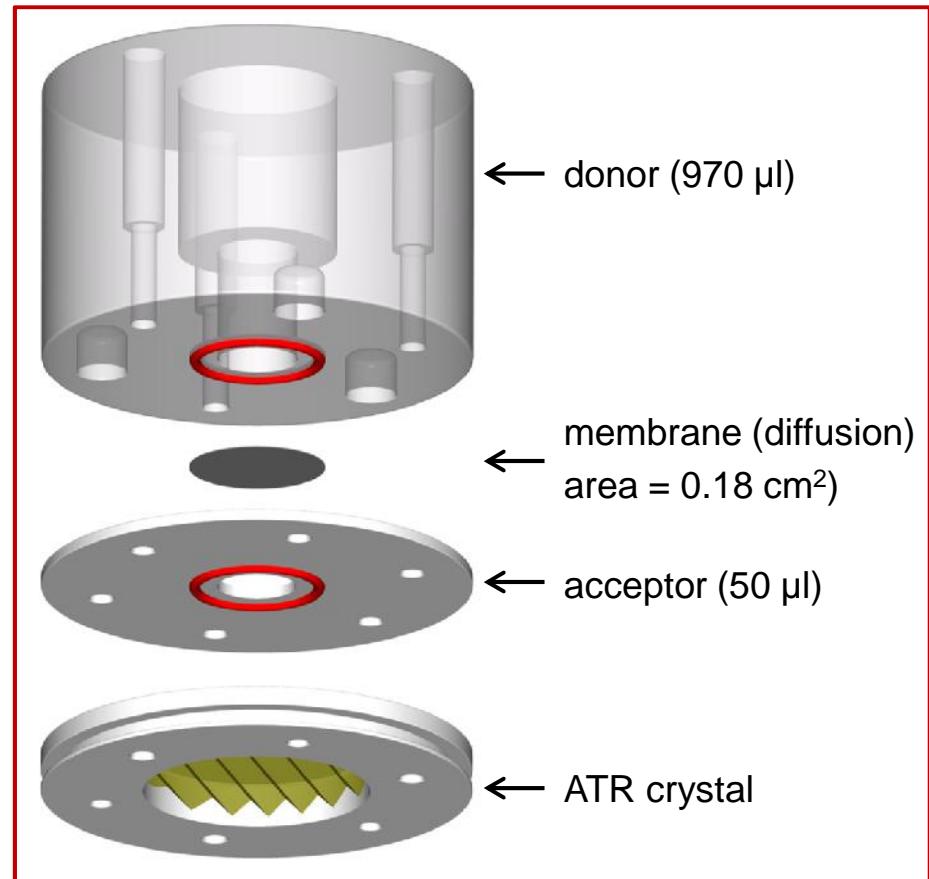
- human skin ex vivo



FTIR-ATR diffusion cell:

- for online measurements

SN2



SN2

Ich hatte eine Diffusionsfläche von 0.0962 cm^2 ausgerechnet...der Durchmesser der Donatoröffnung bzw. des Akzeptors beträgt 3,5 mm

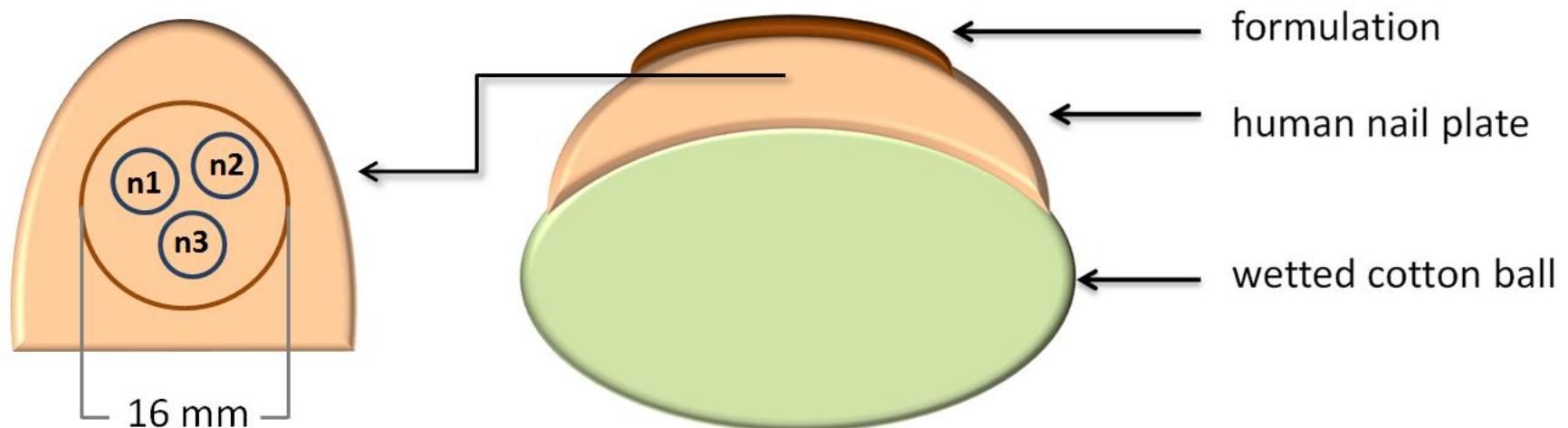
Sandy Naumann; 26.03.2014



Diffusion/Penetration set up

Modified Franz diffusion cell:

- ***Human cadaver nail***
- Slicing of the nail plate using microtome





Diffusion/Penetration set up

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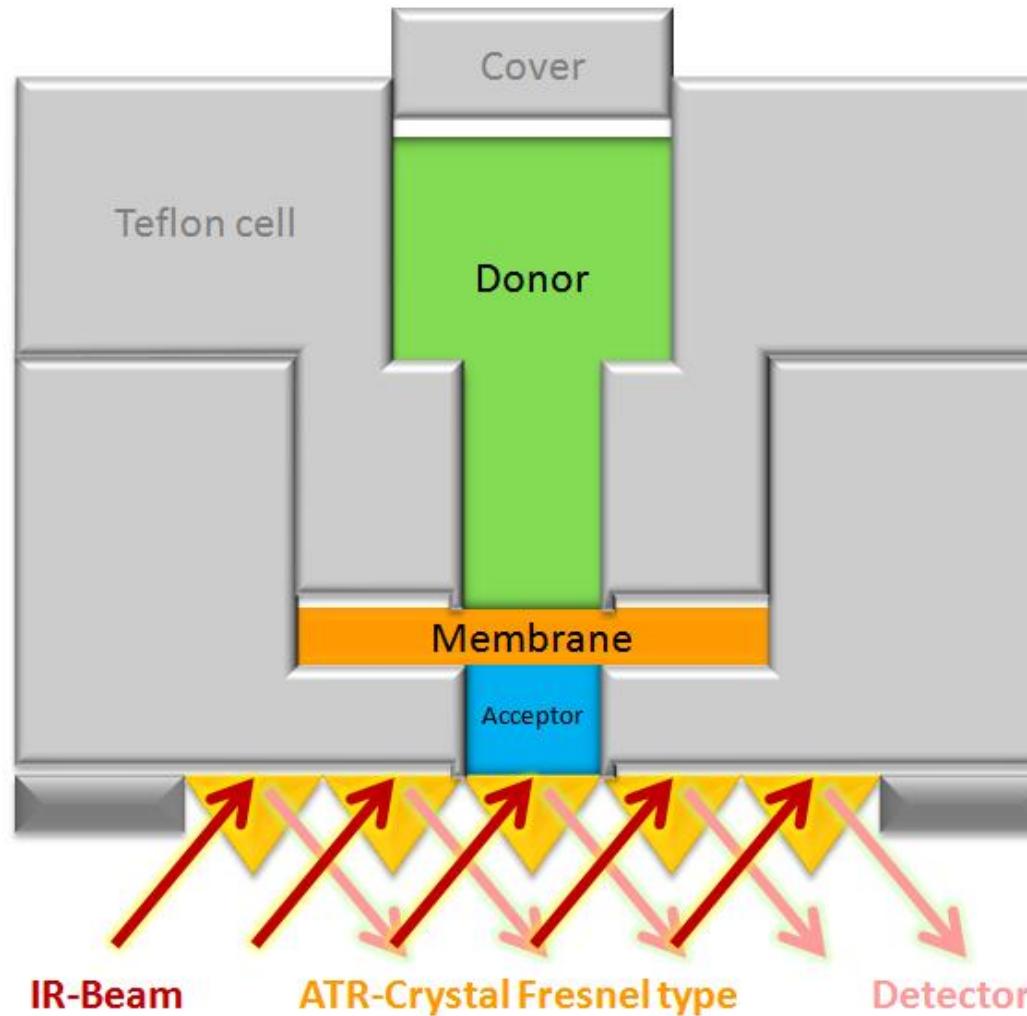
Number of sections and thickness of nail samples of the penetration experiments.

<i>Sections</i>	<i>CCS</i>	<i>S</i>	<i>NL</i>
<i>punch 1</i>	18 x 40 µm	21 x 40 µm	21 x 40 µm
<i>punch 2</i>	23 x 40 µm	26 x 40 µm	26 x 40 µm
<i>punch 3</i>	30 x 40 µm	23 x 40 µm	29 x 40 µm
<i>non-penetrated amount</i>	small filter paper + swab	small filter paper + swab	swab + 60 µl water
<i>acceptor compartment</i>	wetted cotton ball	wetted cotton ball	wetted cotton ball
<i>mean thickness of the nail</i>	947 µm	933 µm	1013 µm



FTIR-ATR diffusion cell

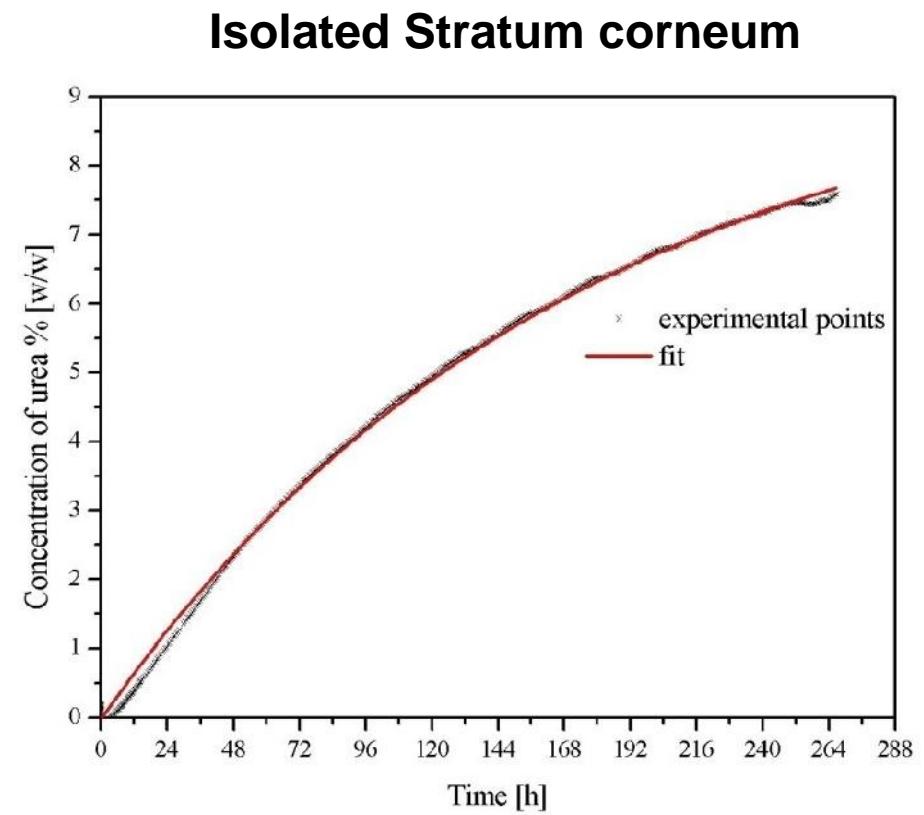
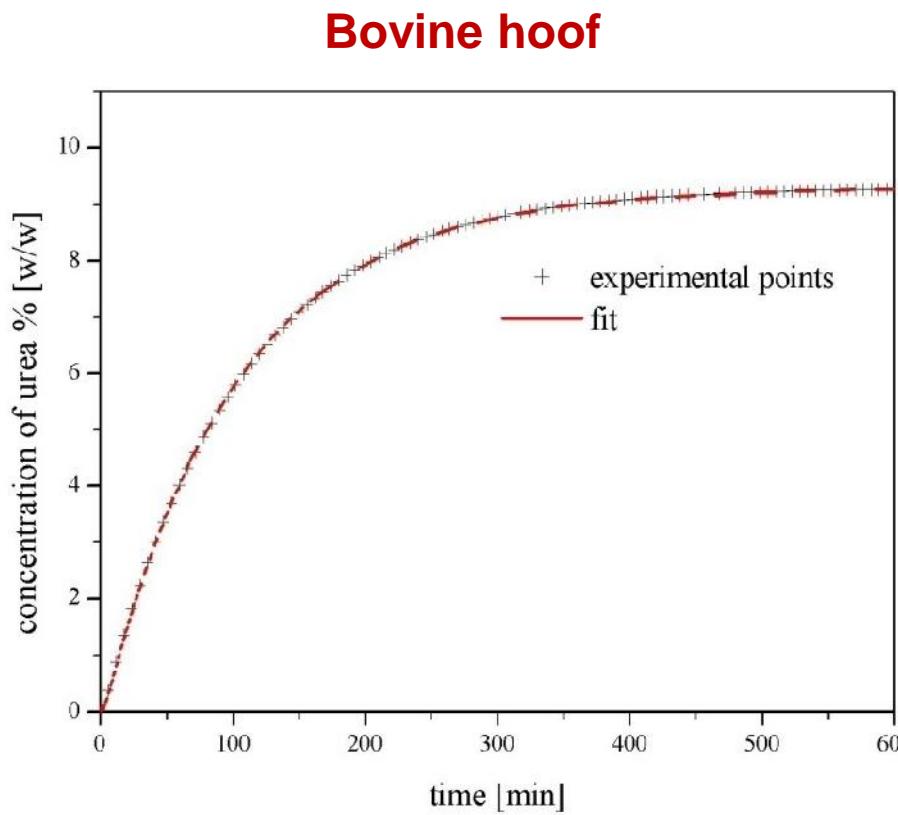
Online determination:





FTIR-ATR cell: Urea diffusion

- **FTIR-ATR diffusion cell:** Fourier transformed IR attenuated total reflection
- **Diffusion of urea:** Hartmann et al. Analyst 129 (2004) 902





Urea diffusion

Diffusion coefficients of urea in human **stratum corneum** and **bovine hoof**:

SC [μm]	D [10^{-10} cm 2 /s]	Rel. SD [%]	Experiment time [h]
24 ± 2	6.04 ± 0.04	0.7	278
30 ± 2	0.63 ± 0.05	7.9	640
36 ± 4	1.88 ± 0.08	4.3	615

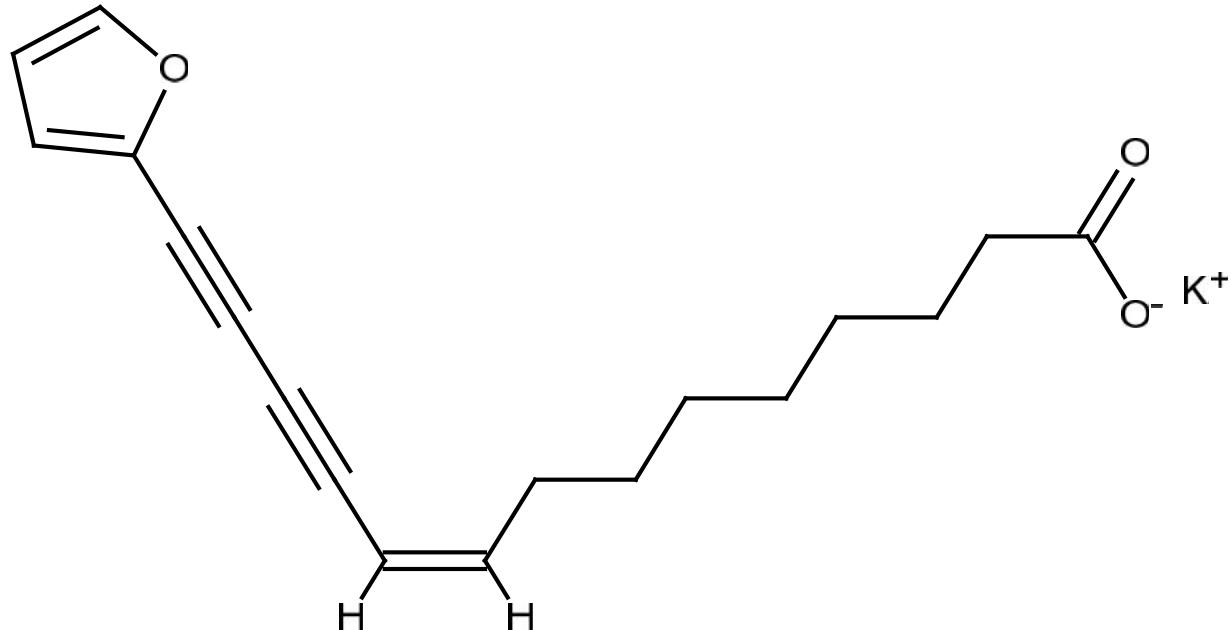
Hoof [μm]	D [10^{-7} cm 2 /s]	Rel. SD [%]	Experiment time [min]
137 ± 9	2.98 ± 0.02	0.67	600
139 ± 5	2.95 ± 0.02	0.68	600
110 ± 4	3.43 ± 0.02	0.58	600



Model drug

Chemical structure of the antifungal **EV-086K**; $M_w = 322.44 \text{ g/mol}$

(Naumann et al. J Control Rel 180 (2014) 60 – 70, **Poster xxxx**)



SN3 Vielleicht möchten Sie noch etwas zum Wirkmechanismus sagen? Ich kann Ihnen gern meine Aufzeichnungen aus der Dissertation zukommen lassen.

Sandy Naumann; 26.03.2014



Model drug

Physicochemical properties of **EV-086K**, $M_w = 322.44 \text{ g/mol}$

Solubilities:

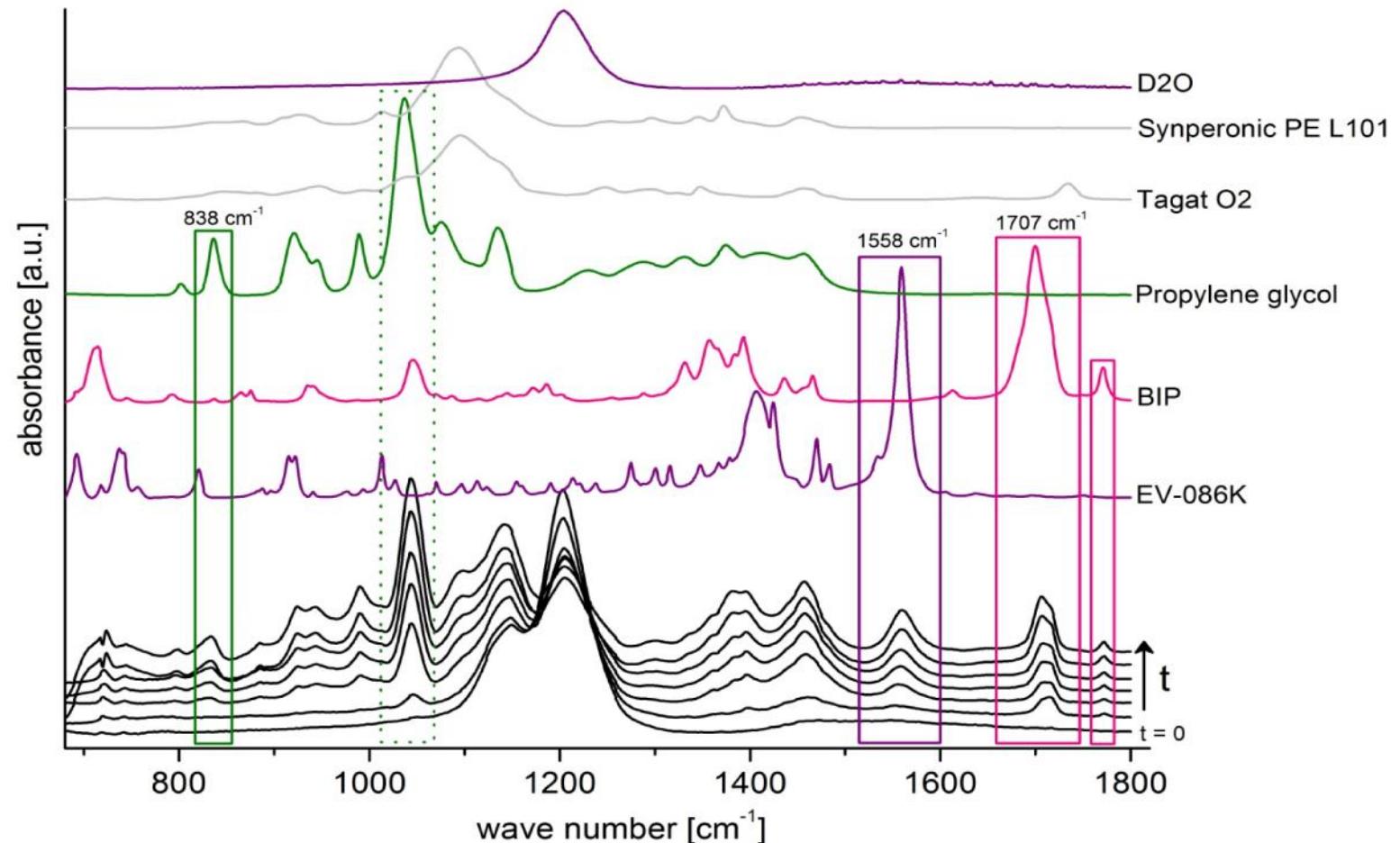
Medium	$c_s [\text{mg/ml}]$	Classification according to Ph. Eur. 7.8
Water	327.9 ± 5.2	freely soluble
Propylene glycol	607.9 ± 67.4	freely soluble
Pentylene glycol	554.9 ± 63.9	freely soluble
Methanol	2152.4 ± 65.2	very soluble
Ethanol	47.3 ± 2.2	soluble
Transcutol® P	1634.2 ± 138.2	very soluble
Soluphor® P	720.2 ± 67.6	freely soluble
Glycerol	0.4 ± 0.1	very slightly soluble
Isopropanol	3.6 ± 0.1	slightly soluble

CMC = 18 µg/ml; log P = 4.54 ± 1.39





FTIR-ATR spectra



FTIR-ATR spectra (colored) of the **single components of the CCS** and FTIR-ATR spectra (black) of the uptake of **EV-086K** and the other ingredients of the CCS into the **acceptor of the diffusion cell** during the penetration experiment (24 hours) through **equine hoof** membranes.



Formulations

How to influence penetration of **EV-086K** into and through the human nails?

Application of the following formulations:

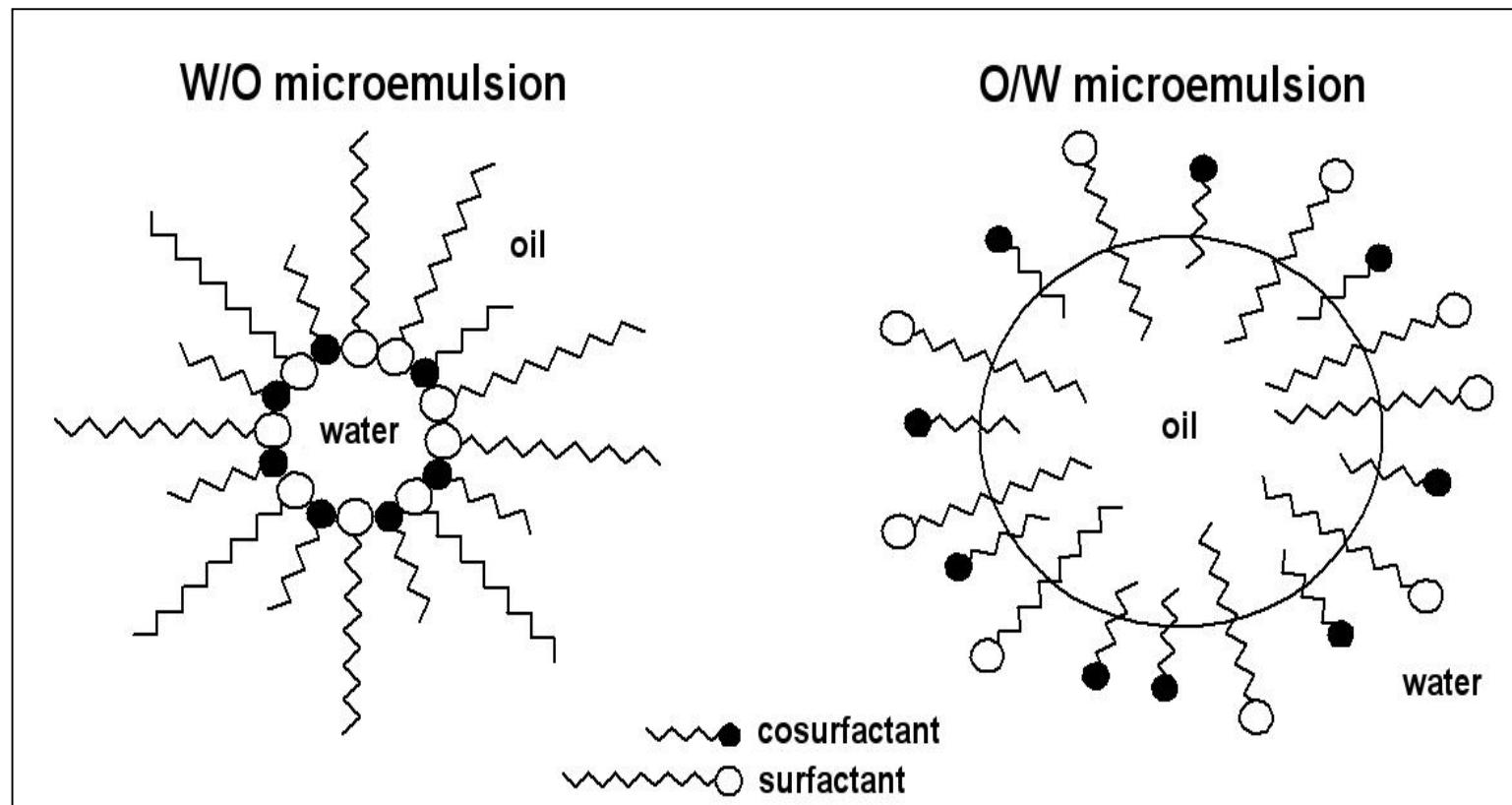
1. **Nail laquer (NL):** Based on dimethylaminoethyl methacrylate, butyl and methyl methacrylate
2. **Colloidal carrier system (CCS):** Radii = 20 - 40 nm, based on the surfactants Tagat® O2 V/ Synperonic™ PE/L and Pelemol® BIP
3. **Solution (S):** Based on water, ethanol and Transcutol® P





Colloidal carrier systems (CCS)

Application of **colloidal carrier systems** (radii = 20 - 40 nm):





Properties of the CCS

Application of colloidal drug carrier systems (CCS):

- Radii = 20 - 40 nm
- Content of surfactants < 20 %
- Physiologically well accepted (nontoxic) surfactants
- Variable over a wide range (O/W- and W/O- systems)
- Thermodynamically stable (very low interface tension)





Penetration of EV-086K: Bovine hoof

Comparison of the parameters of the diffusion experiment using bovine hoof membranes

(mean \pm SD, $p < 0.05$ vs. superscript formulation)

Formulation $c_{EV-086K}$ [%]	n	D_{bovine} [$\times 10^{-9}$ cm 2 /s]	$t_{lag-bovine}$ [min]	linear range [min] $R^2 \geq 0.993$	J_{bovine} [$\mu\text{g}/\text{cm}^2 \text{ min}^{-1}$]	P_{bovine} [$\times 10^{-4}$ cm/min]
NL	12	3	3.0 ± 1.0^S	60 – 156	43.9 ± 10.0	3.7 ± 0.8^S
				163 – 694	15.4 ± 2.3	1.3 ± 0.2
S	5.7	3	1.2 ± 0.5^{NL}	96 – 171	33.8 ± 6.4	5.9 ± 1.1^{NL}
				171 – 1440	11.7 ± 0.4	2.1 ± 0.1
CCS	10	6	11 ± 10.4	19 – 79	76.8 ± 35.9	7.7 ± 3.6
				79 – 324	22.9 ± 8.8	2.3 ± 0.9





Penetration of EV-086K: Equine hoof

Comparison of the parameters of the diffusion experiment using equine hoof membranes

(mean \pm SD, $p < 0.05$ vs. superscript formulation)

Formulation $c_{EV-086K}$ [%]	n	D_{equine} [$\times 10^{-9}$ cm 2 /s]	$t_{lag-equine}$ [min]	linear range [min] $R^2 \geq 0.993$	J_{equine} [$\mu\text{g}/\text{cm}^2 \text{ min}^{-1}$]	P_{equine} [$\times 10^{-4}$ cm/min]	
NL	12	2	4.6 ± 0.8^{CCS}	83 ± 0.1^{CCS}	83 – 190 222 – 1440	36.4 ± 0.7^S 23.2 ± 0.7^S	3.0 ± 0.1 $1.9 \pm 0.1^{S,CCS}$
S	5.7	3	11.3 ± 5.9^{CCS}	57 ± 18	59 – 200 279 – 1440	25.9 ± 4.1^{NL} $4.3 \pm 0.9^{NL,CCS}$	4.5 ± 0.7 $0.8 \pm 0.2^{NL,CCS}$
CCS	10	2	$11.3 \pm 1.2^{NL,S}$	25 ± 6^{NL}	29 – 200	33.3 ± 4.0^S	$3.3 \pm 0.4^{NL,S}$

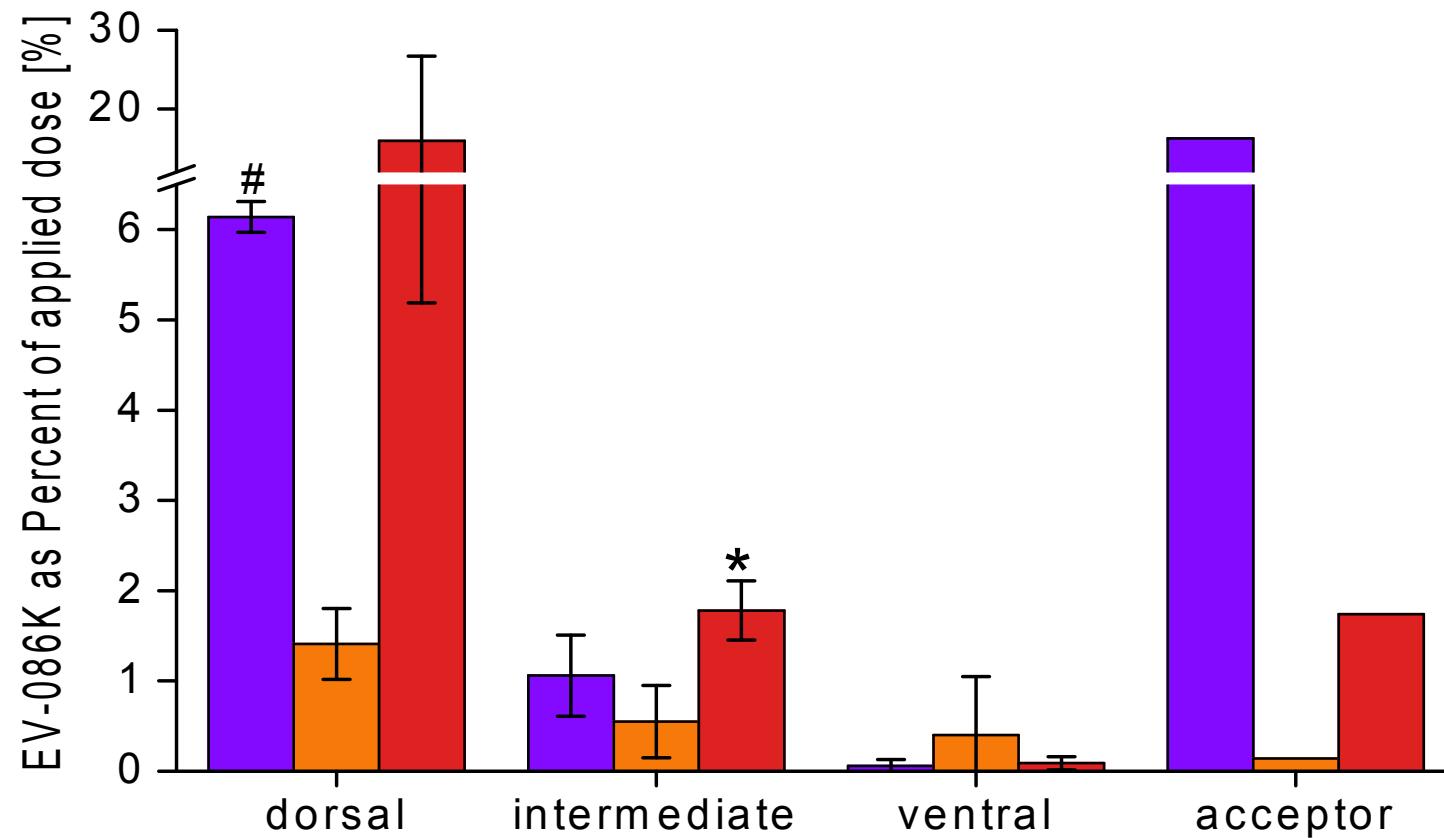




Penetration of EV-086K: Human nail

Comparison of the amounts of EV-086K in % after 24 hours after administration of:

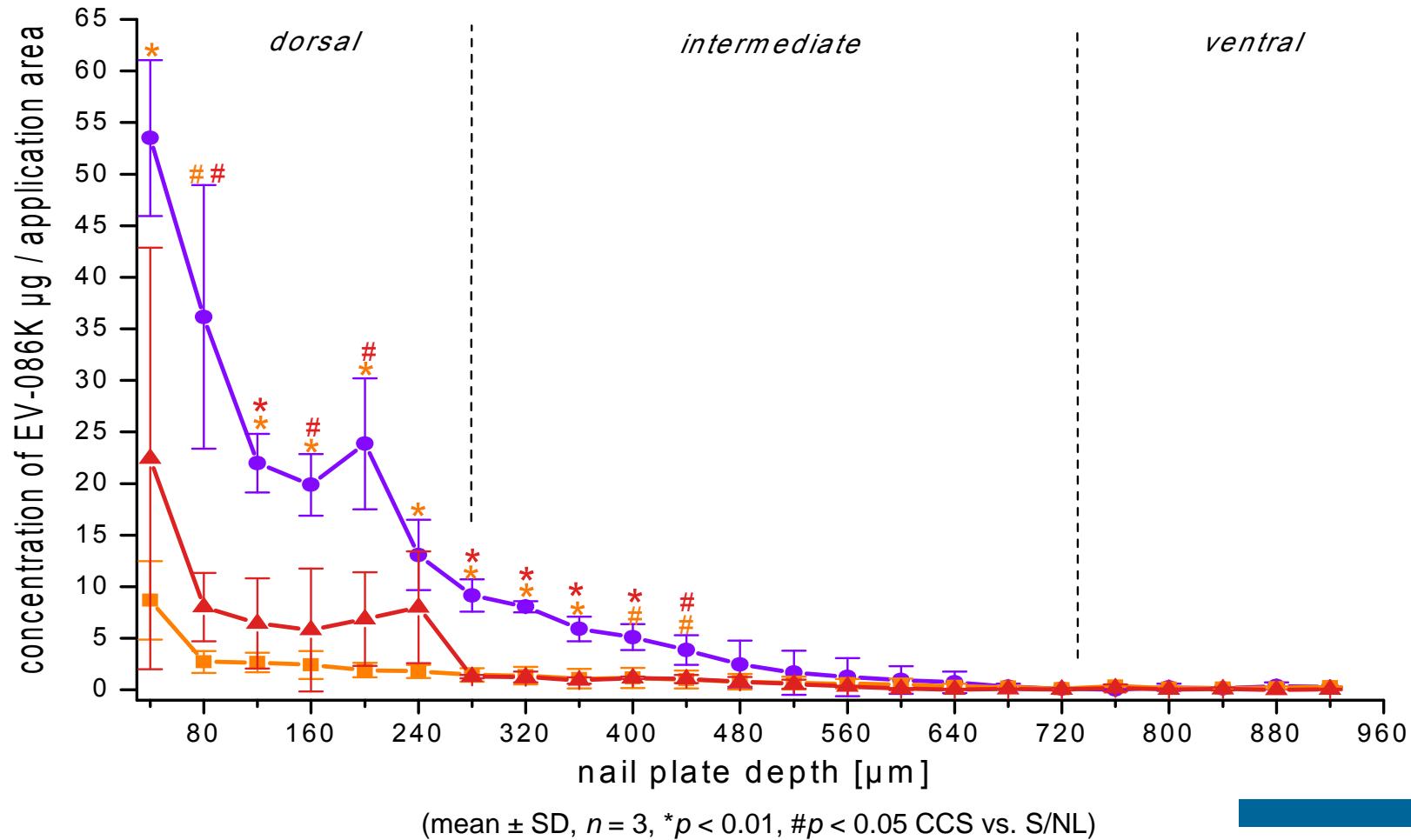
CCS , NL and S , (mean \pm SD, $n = 3$, acceptor: $n=1$; * $p < 0.05$ vs. S; # $p < 0.01$ vs. S).





Penetration of EV-086K: Human nail

Comparison of the penetration profiles of EV-086K in $\mu\text{g}/\text{area}$ after 24 hours after administration of: CCS , NL and S



(mean $\pm \text{SD}$, $n = 3$, * $p < 0.01$, # $p < 0.05$ CCS vs. S/NL)

SN1

In diesem Diagramm sind nur die absoluten Konz. dargestellt und nicht die zur applizierten Dosis.

Sandy Naumann; 26.03.2014



Comparison of EV-086K fluxes

Comparison of the flux values of EV-086K using the different model system:

(Diffusion area of FTIR-ATR diffusion cell: 0.0962 cm^2 ; penetration area of the human nail plates: 2.01 cm^2 , time: 24 hours).

Formulation	$J_{\text{bovine}/20}$ [% /cm 2 h $^{-1}$]	$J_{\text{equine}/20}$ [% /cm 2 h $^{-1}$]	J_{human} [% /cm 2 h $^{-1}$]	$\frac{J_{\text{bovine}}}{J_{\text{human}}}$	$\frac{J_{\text{equine}}}{J_{\text{human}}}$
NL	0.75 ± 0.05	1.25 ± 0.13	0.41 ± 0.22	1.8	3.1
S	1.4 ± 0.07	0.75 ± 0.18	0.05 ± 0.01	28	15
CCS	0.9 ± 0.20	1.05 ± 0.13	0.49 ± 0.01	1.8	2.1

(see Naumann et al. J Control Rel 180 (2014) 60-70)





Conclusions I

1. Human nails can be defined as hydrogel concerning drug diffusion.
2. Onychomycosis is one of the most relevant nail disease.
3. Effective in vitro models are missing for optimizing nail diffusion/penetration from relevant formulations.
4. Diffusion/penetration of the highly lipophilic drug E-086K from different formulations was studied using the methods presented in this lecture.





Conclusion II

5. It could be shown that the equine hoof slices have are simulating the diffusion/penetration conditions into human nails in a better way than the bovine hoof slices.
6. Colloidal carrier systems are the most effective formulation concerning nail delivery of a highly lipophilic drug such as EV-086K.





*Thank you very much
for your attention!*

